Suturing of lacerations of skeletal muscle

Our aim was to compare the biomechanical properties of suturing methods to determine a better method for the repair of lacerated skeletal muscle.

We tested Kessler stitches and the combination of Mason-Allen and perimeter stitches. Individual stitches were placed in the muscle belly of quadriceps femoris from a pig cadaver and were tensioned mechanically. The maximum loads and strains were measured and failure modes recorded. The mean load and strain for the Kessler stitches were significantly less than those for combination stitches. All five Kessler stitches tore out longitudinally from the muscle. All five combination stitches did not fail but successfully elongated.

Our study has shown that the better method of repair for suturing muscle is the use of combination stitches.

Materials and Methods

Direct muscle trauma is common and discontinuity of muscle bellies is an indication for surgery. However, the best suturing technique is not known. Muscle bellies are difficult to repair successfully because the sutures pull out. Some authors have reported healing after repair. These differences may be partly explained by the variation in suturing techniques, of which many have been recommended but few have been compared. For example, a modified Kessler suture, with 5-0 Mersilene, was found to be better than either simple suturing with 2-0 Dexon or simple suturing with a tendon graft. We have previously reported a clinical series of transections of biceps brachii repaired by a combination stitching technique, with a modified Mason-Allen stitch around a perimeter stitch. The combination stitches worked well.

Our aim, therefore, was to compare the maximum loads, strains, and failure modes of muscle bellies sutured with Kessler stitches with those of muscles sutured with combination stitches.

A limb was obtained from an immature female Yorkshire-cross pig weighing approximately 40 kg which had been killed in the course of another study. The experiment was approved by the Animal Care and Use Committee and the institutional review board.

In a pilot study, we selected the best two suturing methods from several methods including a simple stitch, a running simple (epimysium-based, non-core) stitch, a figure-of-eight stitch, a modified Kessler stitch, a vertical mattress stitch, a horizontal mattress stitch (core), a horizontal mattress stitch (inverted, epimysium-based, non-core), a double right-angle stitch and a combination (modified Mason Allen and perimeter) stitch.

The two methods with the highest maximum loads in our pilot study were the Kessler stitch and the combination stitch (Mason-Allen stitch around a perimeter stitch) methods. The performance of the Kessler stitch confirmed that of previous work.

Design of the study. A biomechanical protocol was designed for measuring the passive performance of sutures in lacerations of the muscle belly. We compared individual Kessler stitches and combination stitches. There were five observations in each group. We measured the maximum load, the strain at maximum load and the failure mode.

The limb was refrigerated at -4°C for 43 hours. Quadriceps femoris was dissected from the compartmental fascia taking care to preserve the epimysium. A transverse laceration was made across the belly in an area where no tendon was present. Saline was used to moisten the specimens during testing. For the Kessler stitch group, the sutures were placed around the edge of the laceration using metric size 6 braided polyester sutures Deknatel, Fall River, Massachusetts) (Fig. 1). Different parts of the same specimen were used for the experiment.
including the collection of the pilot data. They were spaced around the epimysium so that they were separate. Modified Mason-Allen stitches were supported by a running interlocking stitch along the border of the epimysium with figure-of-eight knots at one end (Fig. 1). The same suture material was used for all the stitches.

Testing of specimens. A servohydraulic testing machine (model 8521S; Instron Corporation, Canton, Massachusetts) was used in a uniaxial configuration. The construct was preloaded with 5 to 8 N, in the anatomical axis of the muscle, to remove the slack before testing. It was loaded at an elongation rate of 25 mm per minute until failure.

Analysis of data. Data collection software (Series IX, Instron Corporation) recorded the load and strain data as the biomechanical parameters of the performance of the stitches. Maximum load was expressed in newtons and the mm expressed as a percentage. The failure mode was observed directly and recorded.

Statistical analysis. Independent sample t-tests were used for loads and strains and Levene’s test for assessing the quality of variance. The Kolmogorov-Smirnov test confirmed that there was no significant difference between the observed distributions and a normal distribution (p > 0.05) and, therefore, the use of independent sample t-tests was justified. For analysing the mechanism of failure, a 2 x 2 contingency test was used with Fisher’s exact test because of the small sample sizes. A p value < 0.05 was considered to be significant. SPSS (version 11.5; SPSS Inc, Chicago, Illinois) and SigmaPlot (version 9.0; Systat Software, Point Richmond, California) were used for statistical analysis.

Results

Maximum load. The difference between the mean of the Kessler and combination stitches was significant (p < 0.001; Fig. 2). The mean maximum load was 35.1 N (SD 9.4) for
Kessler stitches and 74.0 N (SD 11.3) for combination stitches.

**Strain at maximum load.** The difference between the means was significant ((p = 0.036); Fig. 3). The mean strain at maximum load was 7.9% (SD 2.9) for Kessler stitches and 12.2% (SD 3.7) for combination stitches.

**Failure mode.** There was a significant difference in the failure modes between the groups (p = 0.008). All five Kessler stitches tore out from the muscle. No combination stitch failed since each elongated successfully and reached the maximum preset displacement of 35 mm.

**Discussion**

Our study showed that the maximum loads for combination stitches were more than double those for Kessler. The strain at maximum load and the failure mode were better with the combination stitches.

The suture usually pulls out of the muscle, but in our study we found that the muscle did not fail before reaching the maximum displacement of 35 mm. Overall, the combination of a core stitch (Mason-Allen) and an epimysium-based stitch (perimeter stitch) loaded the muscle better than the core stitch alone (Kessler stitch).

The strength of our study is the comparison of the properties of the initial stitch in muscle lacerations. We are aware that the loads and strains would be higher if our method had allowed further elongation when the results for the combination stitch may have been even better. Our study complements a clinical report in which the combination stitch may have been even better.

Our study showed that the maximum loads for combination stitches were more than double those for Kessler. The strain at maximum load and the failure mode were better with the combination stitches.

The weakness of our study is the limited scope of the model. The effect of cellular healing cannot be considered in cadaver specimens. Tendon repairs have been found to be weakest about 21 days after repair. We did not look at issues such as the size of the suture, the material, the strand number or tendon grafting. Cyclic loading of a repair of the two half bellies was not studied. The sample sizes were small, but using one muscle for testing allowed assessment of the performance of the stitches to be made without intermuscular variability.

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No benefits in any form have been received or will be received from a commercial party related directly or indirectly to the subject of this article.

**References**